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## Mechanosignalling in cartilage: an emerging target for the treatment of osteoarthritis

### AUTHOR(S)

Tom Hodgkinson, Domhnall Kelly, Caroline Curtin, Fergal O'Brien

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1 **Targeting mechanosignalling in cartilage repair: an emerging paradigm in the treatment of**  
2 **osteoarthritis**

3 Tom Hodgkinson<sup>1,\*</sup>, Domhnall C. Kelly<sup>1,2,\*</sup>, Caroline M. Curtin<sup>1,3,4</sup> and Fergal J. O'Brien<sup>1,2,3,4,†</sup>

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5 <sup>1</sup> Tissue Engineering Research Group, Department of Anatomy and Regenerative Medicine, Royal College  
6 of Surgeons in Ireland, St. Stephen's Green, Dublin, Ireland.

7 <sup>2</sup> Centre for Research in Medical Devices (CÚRAM), National university of Ireland, Galway, Ireland.

8 <sup>3</sup> Advanced Materials and Bioengineering Research Centre (AMBER), RCSI and Trinity College Dublin  
9 (TCD), College Green, Dublin, Ireland.

10

11 <sup>4</sup> Trinity Centre for Biomedical Engineering, Trinity Biomedical Sciences Institute, Trinity College Dublin,  
12 College Green, Dublin, Ireland.

13

14 **†Corresponding Author**

15 Prof. Fergal J. O'Brien

16 Email: [fjobrien@rcsi.com](mailto:fjobrien@rcsi.com)

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21 **Abstract**

22 Mechanical stimuli play a fundamental role in articular cartilage health and disease. Chondrocytes respond  
23 to the physical properties of the extracellular matrix (ECM) and the mechanical forces exerted during joint  
24 loading. In osteoarthritis (OA), catabolic processes degrade the functional ECM, while the composition and  
25 viscoelastic properties of the matrix produced by chondrocytes are altered. The abnormal loading  
26 environment created propagates cell dysfunction and inflammation. Chondrocytes sense their physical  
27 environment via an array of mechanosensitive receptors and channels, which in turn activate a complex  
28 network of downstream signalling pathways and regulate a plethora of cell processes central to OA pathology.  
29 This review focuses on recent advances in the understanding of the complex role of specific  
30 mechanosignalling mechanisms in cartilage health and OA, highlighting key molecular processes that can  
31 be therapeutically targeted to interrupt pathological feedback loops. The potential for combining these  
32 mechanosignalling targets with the rapidly expanding field of smart mechanoresponsive biomaterials and  
33 delivery systems will be discussed as an emerging paradigm in OA treatment. The continued advancements  
34 in this field have the potential to enable restoration of healthy mechanical microenvironments and signalling  
35 through the development of precision therapeutics, mechano-regulated biomaterials and drug systems in the  
36 near future.

37

38 **Key Points**

39

40 • Mechanical forces are a critical environmental factor in maintaining joint homeostasis, determining  
41 cell phenotype, inflammatory responses and a tightly regulated anabolic-catabolic signaling axis  
42 essential to cartilage homeostasis.

43

44 • Chondrocytes sense their mechanical environment through numerous direct and indirect  
45 mechanisms that regulate cell function in health and degenerative diseases, such as osteoarthritis.

46

47 • Targeted inhibition of mechano-inflammatory signalling pathways or restoration of functional  
48 chondroprotective extracellular matrix environments in OA may prevent ECM degradation and  
49 promote reparative anabolic processes.

50

51 • Development of self-regulating and mechanically responsive biomaterials and drug delivery systems  
52 offer advanced 'on-demand' therapeutic approaches for the treatment of OA.

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## 57 **Introduction**

58 Mechanical signalling is a critical mediator of numerous physiological and pathophysiological processes in  
59 the cells and tissues of the joint. In cartilage, chondrocytes synthesize, and are surrounded by, a highly  
60 specialized extracellular matrix (ECM) that allows low friction movement and protects the tissue during  
61 mechanical loading. In healthy cartilage, the mechanical forces generated by movement are an essential  
62 component of maintaining the homeostatic balance of chondrocyte-mediated ECM deposition and re-  
63 modelling – a dynamic, continuous process of adaptation to the local mechanical environment, involving both  
64 sensation and transduction of forces. However, though some movement is required for healthy cartilage,  
65 excessive mechanical loading is also a key risk factor in the pathogenesis and progression of osteoarthritis  
66 (OA). Decades of research have demonstrated that the role of mechanical loading in the pathobiology of OA  
67 goes beyond tissue ‘wear-and-tear’ and is in fact a dynamic driving force in the disease, through the activation  
68 of mechanoresponsive cell signalling (mechanosignalling) and resultant production of inflammatory  
69 mediators and catabolic enzymes.<sup>1,4</sup> This pathological signal transduction, which can be viewed as a  
70 corruption of chondrocyte mechano-adaptive processes, occurs when chondrocytes experience excessive  
71 physical forces, or when the chondroprotective ECM is compromised. In the latter, inadequate distribution of  
72 loads means that even within normal physiological ranges excessive stress can be exerted on chondrocytes.  
73 In addition, loss of key ECM molecules and structures also significantly impacts mechanically controlled  
74 chondro-protective mechanisms.<sup>5,6</sup>

75         The pathological changes in the cartilage ECM in OA, which include degeneration of the functional  
76 matrix (most notably type II collagen and proteoglycans), loss of tissue hydration and production of incorrect  
77 fibrous ECM, occur concomitantly with aberrant chondrocyte proliferation, senescence, inflammation, and  
78 hypertrophy.<sup>7</sup> Dysregulation of mechanosignalling appears to play a central role in these related processes  
79 and the phenotypic drift of chondrocytes seen in OA. Although the mechanisms by which degenerative or  
80 reparative signalling programs are initiated within the cell are not fully elucidated, key molecular pathways  
81 and signalling mechanisms have been identified. In OA, targeting these pathways is an emerging strategy to  
82 reduce the release of the proinflammatory cytokines and catabolic enzymes that drive the progression of the  
83 disease.<sup>8,9</sup> Further to this, recent work demonstrates the direct interaction of mechanosignalling and  
84 inflammatory mediators, highlighting the potential for mechanobiology approaches to simultaneously boost  
85 repair and reduce mechano-inflammation.<sup>10</sup> It is likely that correction of pathological mechanosignalling,  
86 either through adjustment of the cellular mechanical environment or through control over mechanosignalling,

87 will enhance the clinical impact of locally delivered anabolic factors that have shown promise, for example  
88 FGF18.<sup>11</sup>

89 Regenerative biomaterials offer the opportunity to restore repair-stimulating mechanical  
90 environments while potentially, through additional functionalisation, delivering disease-modifying OA drugs  
91 (DMOADs) or nucleic acids. Systems under development can provide sophisticated control over this delivery,  
92 including stimuli-responsive release systems, highlighting the potential for closed-loop therapeutic delivery.<sup>12</sup>  
93 Similarly, synthetic gene circuits that respond to OA-associated stimuli, e.g., inflammatory signalling, by  
94 upregulating the production of DMOADs represent an exciting development to enable in situ self-regulating  
95 therapeutic cell reprogramming.<sup>9</sup>

96 In this review, we focus on recent advances in the understanding of the complex role of specific  
97 mechanosignalling mechanisms in chondrocytes in healthy and OA cartilage. We highlight several key  
98 molecular processes with therapeutic potential and discuss strategies to target these to interrupt pathological  
99 feedback loops, including the potential for combining these mechanosignalling targets with the rapidly  
100 expanding field of smart mechanoresponsive biomaterials and delivery systems.

101

## 102 **Cartilage mechano-adaptation in health and disease**

103 Articular cartilage has a structure that is highly specialised for low friction movement and weight bearing.  
104 Cartilage itself can be subdivided into three overlapping zones moving from the subchondral bone towards  
105 the articulating surface- the deep calcified zone, the intermediate zone and the superficial zone.<sup>13</sup> Within  
106 these zones, the ECM composition and architecture reflect the forces they experience during movement. In  
107 the deep zone, to resist compressive loads type II collagen fibres are thick and arranged perpendicular to the  
108 joint surface while proteoglycan concentrations are high to promote water retention. The intermediate zone  
109 experiences compressive and shear forces, and type II collagen fibres are arranged randomly to resist forces  
110 from a number of directions. In the superficial zone, chondrocytes and type II collagen fibres are orientated  
111 transversely to disperse shear forces during articulation and secrete proteoglycan 4 (PRG4) for lubrication  
112 (Figure 1).<sup>13</sup> On the tissue scale, the physical properties of cartilage are determined by the composition of  
113 the ECM - a predominantly type II collagen network trapping high concentrations of proteoglycans (e.g.  
114 aggrecan, lubricin, perlecan) and glycosaminoglycans (GAGs) (e.g. hyaluronan).<sup>14-16</sup> These proteoglycans  
115 and GAGs impart a fixed negative charge on the ECM, promoting water retention and conferring remarkable  
116 shock-absorbing and low-friction properties. Tissue compression forces this interstitial fluid from the tissue,  
117 which upon unloading returns through charge interactions. Concurrently, hydrostatic pressure generated by  
118 ECM obstruction of interstitial fluid movement protects the tissue from compressive forces.<sup>15</sup> Chondrocytes

119 therefore experience a range of loading modes, often simultaneously (compression, stretch, shear, pressure)  
120 through the transducer of this ECM. In combination with magnitude and frequency of force, the integrity of  
121 the ECM plays a significant role in determining if an experienced load initiates catabolic signalling cascades  
122 in tissue resident chondrocytes. Evidence indicates that ECM degradation not only affects the transmission  
123 of forces across the tissue but can alter the type of loading experienced by a chondrocyte in a particular zone,  
124 significantly impacting cell responses.<sup>2</sup>

125 The matrix in which chondrocytes reside does not have a homogenous structure and composition.  
126 Surrounding chondrocytes, a distinct region termed the pericellular matrix (PCM) has perhaps the most  
127 significant influence on cell mechanotransduction. Together with the cell itself, this region, which is around  
128 2-4  $\mu\text{m}$  thick, forms the structural, functional and metabolic unit commonly referred to as the 'chondron'.<sup>17</sup>  
129 The PCM can be around an order of magnitude softer than the bulk tissue ECM (0.04-0.1 MPa and 0.1-2MPa  
130 respectively) and is characterized by the presence of type VI collagen but also contains other important  
131 components including perlecan, aggrecan, hyaluronan, biglycan, type IX collagen, laminin, and  
132 fibronectin.<sup>17,18</sup> Moving outwards from the cell the PCM integrates with the territorial matrix (TM), a region  
133 characterised by a network of tightly packed fine, fibrillar collagen, proteoglycan and fibronectin.<sup>19-21</sup> In turn  
134 the TM integrates with the interterritorial matrix (ITM) or the bulk tissue ECM (Figure 1). Though the integrity  
135 of all of these ECM regions is important for tissue function, the PCM directly modulates the forces  
136 experienced by the cell. Therefore, chondrocytes effectively respond to mechanical stresses either 'directly'  
137 through sensing PCM deformation via cell-matrix adhesions and/or cell sensory structures, or 'indirectly'  
138 following the mechanically induced release of sequestered growth factors and their interaction with cell  
139 receptors (Figure 2).

140 Considering this function, it is perhaps no surprise that the PCM, and in particular the destruction of  
141 the PCM, has been implicated in playing a pivotal role in disease.<sup>22</sup> Indeed, PCM degeneration is one of the  
142 earliest events in OA, altering both the transmittance and mode of mechanical forces experienced by  
143 chondrocytes.<sup>23,24</sup> It is interesting to note that experimental and *in silico* models show that the forces  
144 experienced by chondrocytes across various species are comparable and independent of animal mass due  
145 to variation in PCM/ ECM properties between species.<sup>25,26</sup> When a mechanical stimulus is outside these  
146 thresholds, ECM remodelling is initiated. Targeting chondrocyte mechanosensing offers the opportunity to  
147 re-tune cell thresholds in disease to re-establish the dynamic homeostatic balance.

148 Alterations in the composition and architecture of the PCM and TM lead to altered bioavailability of  
149 sequestered growth factors.<sup>27-30</sup> Following deformation or destruction, ECM sequestered factors are released

150 to interact with cell membrane receptors, activating downstream intracellular signalling. A well-studied  
151 example of this is PCM/ TM involvement in FGF signalling (recently reviewed in<sup>31</sup>).<sup>27,32-35</sup> All FGFs depend  
152 on heparin sulphate to act as an obligate co-receptor to bind, dimerise and activate receptors (FGFRs).<sup>31</sup> In  
153 the PCM and TM, FGFs bind to perlecan, a heparin sulphate proteoglycan and form an FGF-reservoir that is  
154 released to activate FGFRs on mechanical stimulation. FGF signalling can activate multiple intracellular  
155 signalling pathways including PKC (protein kinase C), MAPK (Ras-Mitogen-activated protein kinase) and  
156 PI3K (phosphoinositide 3-kinase)/ AKT (protein kinase B).<sup>31</sup> A healthy PCM/ TM composition is likely to have  
157 a significant impact on both the availability of sequestered FGFs and the type of FGF present, as family  
158 members exhibit differing affinities for heparin sulphate binding. With FGFs, the balance between the  
159 deleterious and beneficial effects of signalling is dependent on the specific family members and receptors  
160 activated.<sup>36</sup> Notably FGF18 (sprifermin), which activates FGFR3 is the only FGF therapy undergoing clinical  
161 trials and has shown encouraging results by increasing cartilage thickness and reducing loss through intra-  
162 articular injection in OA (Figure 2A).<sup>37-39</sup>

163 The activity of several other growth factor families have mechanical elements to their activity and  
164 regulation including members of the TGF $\beta$  superfamily, in which mechanical stress activates TGF $\beta$  signalling  
165 in an integrin-dependent manner (discussed further below).<sup>40</sup> Further understanding of how the initiation of  
166 anabolic or catabolic/ inflammatory signalling is regulated, the signalling proteins released under  
167 injurious/non-injurious conditions and their impact on the anabolic-catabolic axis of cartilage tissue will  
168 provide valuable information to guide the development of pharmacological treatments for OA. Below, we  
169 discuss several key chondrocyte mechanosignalling mechanisms including, integrins,<sup>41-43</sup> mechanosensitive  
170 ion channels,<sup>44-49</sup> cytoskeletal and nucleoskeletal constituents,<sup>50</sup> and the primary cilium.<sup>51-54</sup>

171

### 172 ***Integrin-mediated mechanosignalling***

173 Integrins, the most well-studied of the cell adhesion molecules, are key components in determining cell  
174 responses to their environment. Their activity is tightly controlled through both biochemical and mechanical  
175 regulatory pathways (reviewed in<sup>55-59</sup>). Briefly, upon ligand binding, integrins undergo conformational  
176 changes, exposing regions in their cytoplasmic tails that promote binding to the actin cytoskeleton and  
177 integrin adhesion complex formation.<sup>60,61</sup> The maturation of these nascent adhesion complexes into focal  
178 complexes, focal adhesions, and fibrillar adhesions is tightly regulated.<sup>59</sup> Integrin-mediated force generation  
179 and mechanotransduction occurs through the 'molecular clutch' mechanism<sup>62</sup> in a substrate stiffness and  
180 integrin type-dependent manner (reviewed in <sup>59</sup>) (Figure 2B).<sup>63,64</sup> In articular cartilage, several integrin



181 heterodimers are present including  $\alpha 1\beta 1$ ,  $\alpha 5\beta 1$ ,  $\alpha 10\beta 1$ ,  $\alpha 11\beta 1$  and  $\alpha V\beta 1$ , with a weaker expression of  
182  $\alpha 3\beta 1$  and  $\alpha V\beta 3$ .<sup>65-67</sup> The integrin profile of OA chondrocytes is altered and difficult to interpret. For example,  
183 the expression of  $\alpha 1\beta 1$ ,  $\alpha 3\beta 1$ ,  $\alpha 2\beta 1$ ,  $\alpha 4\beta 1$  and  $\beta 2$  is increased but the full implications of this are currently  
184 unclear.<sup>68-70</sup> The expression of some integrin subunits is responsive to mechanical stimulation (e.g.,  $\alpha 5$ ,  
185 which increases)<sup>71</sup> and several have been linked with both healthy and pathological chondrocyte  
186 mechanosignalling. Recently, a critical role for  $\alpha V$  integrin in the activation of TGF $\beta$  signalling in regions of  
187 mechanical stress in OA cartilage was demonstrated,<sup>40</sup> revealing one mechanism by which pathological ECM  
188 destruction is localised in the tissue. In regions of high mechanical stress in the cartilage, generated by altered  
189 subchondral bone architecture in OA, talin-mediated increases in cytoskeleton contractile forces and  
190 chondrocyte stiffness trigger  $\alpha V$ -mediated activation of TGF $\beta$ . Through this mechanism, regions of TGF $\beta$   
191 activation are correlated with regions of high mechanical stress, where TGF $\beta$  activation dysregulates  
192 chondrocyte metabolism and homeostasis, driving ECM degradation. Knockout of  $\alpha V$  integrin in mice  
193 significantly attenuated this TGF $\beta$  activation and downstream ECM degradation. Other interesting integrin  
194 expression profiles include the  $\alpha 10$  and  $\alpha 11$  subunits and  $\beta 1$ -containing integrins.<sup>69,72-76</sup> Integrin  $\alpha 10$  is the  
195 dominant collagen-binding integrin in healthy chondrocytes,<sup>77,78</sup> while  $\alpha 11$ , which is also collagen-binding, is  
196 expressed at low levels.<sup>65,67,79</sup> In contrast,  $\alpha 11$  is increased in OA cartilage and also correlates with poorer  
197 chondrogenic differentiation of mesenchymal stem cells.  $\alpha 10$  expression is also upregulated by  
198 chondroprotective factors like FGF2 and BMP2, while  $\alpha 11$  is increased by TGF $\beta$ .<sup>65,80</sup> Mechanistic details of  
199 how these integrin subunits exert their effect on cell phenotypes is yet to be determined, though a link to cell  
200 stiffness and cytoskeletal contractility seems likely. Clearly, the significant influence of these integrins and  
201 others on chondrocyte behaviour make them attractive therapeutic targets in the treatment of OA. For this,  
202 the “repurposing” of integrin receptor antagonists that are currently available or undergoing clinical  
203 examination may be an attractive approach. For example, Cilengitide, a selective inhibitor of integrin  $\alpha V\beta 3$   
204 and  $\alpha V\beta 5$ , currently in clinical trials for the treatment of glioblastoma is capable of suppressing inflammatory  
205 (IL-1 $\beta$ , TNF- $\alpha$ ) and catabolic mediators (MMP3, MMP13) in chondrocytes.<sup>81</sup>

206

### 207 ***Cytoskeletal and nucleoskeletal elements***

208 The cytoskeleton has a significant impact on mechanotransduction and plays a fundamental role in  
209 physiological and pathological chondrocyte phenotypes.<sup>50</sup> The actin cytoskeleton undergoes reorganisation  
210 with deformative (e.g., compression) and non-deformative loading (osmotic, hydrostatic pressure), and

211 disruption of F-actin is associated with altered cell viscoelastic properties and nuclear deformation following  
212 compression.<sup>82-85</sup> Treatment with thymosin B4, an inhibitor of F-actin polymerisation, results in elevated  
213 expression of catabolic mediators, leading to increased cartilage catabolism with mechanical stress.<sup>86</sup>  
214 Cytoskeletal elements are abnormally distributed and assembled (or even absent altogether) in OA  
215 chondrocytes, compromising cell metabolic activities and biomechanical integrity.<sup>87,88</sup> Moreover, in culture  
216 the application of an anabolic cyclical loading regime alone is unable to reverse these cytoskeletal changes,  
217 suggesting a combined intervention approach is required.<sup>88</sup>

218 Direct mechanotransduction in part relies on a physical link between the ECM, cytoskeleton and the  
219 nucleus. The cytoskeleton transmits external forces to the nucleus via linker of nucleoskeleton and  
220 cytoskeleton (LINC) complexes associated with nuclear lamins. These deformations influence chromatin  
221 dynamics, epigenetics, and gene transcription (Figure 2B).<sup>89,90</sup> Dysregulation of nuclear mechanosensing  
222 has been observed recently in OA subchondral bone, where it has a role in HDAC epigenetic regulation of  
223 MSC osteogenic potential.<sup>91</sup> Mechanically, cellular tension developed by the cytoskeleton also directly  
224 regulates YAP nuclear translocation, where it can promote the transcription of YAP-target genes. This direct  
225 mechanical activation has been demonstrated in 2D, where cytoskeletal tension stretches the cell nucleus  
226 and nuclear pores facilitating YAP movement into the nucleus.<sup>92</sup> This direct mechanism of nuclear entry may  
227 have significant implications for controlling YAP activity in the altered mechanical environment of the OA.

### 228 ***The chondrocyte channelome***

229 Chondrocytes express a diverse array of ion channels and porins collectively referred to as the 'chondrocyte  
230 channelome' (Reviewed in <sup>45,49</sup>). The activity of channelome proteins is associated with fluctuations in ion  
231 signalling, one of the earliest cellular events in chondrocyte responses to various modes of mechanical  
232 stimulation. Ion channels can be classified based on their gating mechanisms such as voltage, ligand, or  
233 mechanically-gated. While each type of channel can be found in the chondrocyte channelome, mechanically-  
234 gated ion channels are of particular interest as they are capable of inducing rapid mechanosensory  
235 transduction. Calcium signaling ( $Ca^{2+}$ ), a ubiquitous second messenger, has a key role in activating multiple  
236 intracellular signaling pathways in mechanotransduction (Figure 2B, 2C). Any initial ion influx can also be  
237 amplified further by the subsequent release of ions from intracellular stores. In cartilage, recent work has paid  
238 particular focus to members of the vallinoid subfamily of transient receptor potential (TRPV) channels, which  
239 are regulators of intracellular  $Ca^{2+}$  concentration in non-excitabile cells. While chondrocytes express various  
240 TRP channels, the TRPV4 non-specific cation channel has gained interest due to its role in controlling the

241 mechano-osmotic transduction cascade (Figure 2B, 2C).<sup>46,47,93</sup> TRPV4-mediated intracellular Ca<sup>2+</sup> signaling  
242 is a key mechanosignalling pathway in chondrocytes and is involved in regulation of ECM biosynthesis.<sup>47</sup>  
243 Deletion of TRPV4 in mice results in severe OA-like presentations,<sup>46</sup> while strikingly, loss of TRPV4 in  
244 chondrocytes prevents age-related OA development but not mechanical load-dependent OA.<sup>94</sup> These  
245 anabolic roles for TRPV4 suggest it is a promising therapeutic target. In other mechanosensitive cells, the  
246 TRP proteins, TRPA1 and TRPP2, also have well-established mechanosensory properties and appear likely  
247 to be involved in chondrocytes.<sup>95</sup>

248 While physiological loading can induce an anabolic response in chondrocytes through the activity of  
249 TRPV4 ion channels, another family of mechanosensitive ion channels are implicated in the  
250 mechanotransduction of injurious mechanical stimuli. Piezo channels, specifically Piezo 1 and 2, are cation  
251 permeable ion channels also involved in chondrocyte mechanotransduction (Reviewed further in <sup>96</sup>). Piezo 1  
252 and 2 are distinct from other ion channels in that they consist of 4 transmembrane helical bundles termed  
253 Piezo repeats, which together form flexible propeller blade-like structures. Both Piezo 1 and 2 are present in  
254 chondrocytes, providing high strain mechanosensitivity and the ability to respond to ‘hyperphysiological’  
255 levels of mechanical stress.<sup>97</sup> Briefly, high strain (compressive loading >45% strain) increases Ca<sup>2+</sup> influx via  
256 Piezo channels. Knockdown of either Piezo1 or 2 prevents mechanically induced Ca<sup>2+</sup> transients, suggesting  
257 a synergistic action. Inhibition of Piezo activity with GsMTx4 (a Piezo 1/2 blocking peptide) protects  
258 chondrocytes from mechanically induced cell death, highlighting their therapeutic potential.<sup>96,97</sup>

### 259 **Primary cilia**

260 The primary cilium is a non-motile cellular organelle, which protrudes from the cell surface and contains a  
261 high concentration of mechanosensory machinery and receptors. In chondrocytes, the primary cilia have an  
262 important role in mechanotransduction (Figure 2C).<sup>51,98</sup> Primary cilia exhibit cartilage zone dependent  
263 variation (in both occurrence and length, which both increase with distance from the articulating surface),  
264 which is thought to be as a result of the different stress, strain, and fluid flow experienced throughout each  
265 zone.<sup>51</sup> Interestingly, cilia length and the percentage of ciliated chondrocytes in cartilage have been shown  
266 to increase with OA severity. Additionally, the orientation of OA chondrocyte primary cilia is observed to be  
267 towards the articular surface rather than away as is observed in healthy chondrocytes.<sup>51</sup> In primary cilia  
268 knockouts (*Col2a1Cre/ift88<sup>fl/fl</sup>* transgenic mice) cartilage stiffness is decreased while, tissue thickness and  
269 the expression of several OA markers (*COLX*, *RUNX2*, *MMP13*, *ADAMTS5*) are increased.<sup>53,99</sup> Further,  
270 transgenic mice with mutant Polaris, an essential cilia protein, fail to initiate mechanosignalling and

271 compression of IFT88(orpk) mutant chondrocytes (that lack primary cilia) does not initiate intracellular Ca<sup>2+</sup>  
272 signaling, ECM synthesis or ATP release.<sup>95,100,101</sup> The localisation of mechanosensors to the primary cilia  
273 facilitates the mechanical activation of purinergic signalling in the form of ATP and intracellular Ca<sup>2+</sup>  
274 release.<sup>102</sup> This ATP release is mediated by the mechanically stimulated opening of hemichannels  
275 (connexons), present in high densities in the primary cilia, and is linked with several anabolic activities  
276 including an increase in proteoglycan production and cell proliferation.<sup>102-105</sup>

## 277 **Mechanotherapeutics for the treatment of osteoarthritis**

278 Mechanotherapeutics originally referred to the use of physical therapy to treat a disease but now  
279 encompasses interventions that target molecular, cellular and tissue level mechanosignalling to repair tissue  
280 damage or treat disease.<sup>106,107</sup> In short, mechanotransduction can be targeted in a therapeutic manner to  
281 either promote anti-catabolic, anabolic pathways and repair processes, or to block the pathways central to  
282 OA. However, underlying the complex nature of OA pathogenesis is an equally complex signalling network.  
283 For example, a study aimed at characterising the response of articular cartilage explants to mechanical injury  
284 revealed the significant regulation (>2 fold change) in 690 genes.<sup>108</sup> These pathways are implicated in  
285 regulating inflammation, production of catabolic and degradative enzymes (*MMPs*, *ADAMTSs*), cellular  
286 apoptosis and bone dysfunction within the joint. In the following sections, we highlight some of the prominent  
287 mechanosignaling pathways that have been implemented in the pathogenesis and progression of OA and  
288 how these pathways might be targeted therapeutically (Figure 3).

289

## 290 ***The Mitogen-Activated Protein Kinase (MAPK) Pathway***

291 The mitogen-activated protein kinases (MAPKs) play a key role in the regulation of various cell signaling  
292 pathways that are implicated in cellular proliferation, matrix synthesis, survival and mediation of pain.<sup>109</sup> In  
293 chondrocytes, MAPKs are involved in regulating gene expression in response to mechanical stimulation.  
294 Activation of ERK1/2, P38 MAPK and the SAPK/ERK kinase 1 (SEK1) occurs following compression.<sup>110</sup>  
295 Furthermore, integrin activation through matrix fragments activates MAP kinases and results in the  
296 upregulation of catabolic signalling. As previously discussed,  $\alpha 5\beta 1$  mediates matrix degradation induced by  
297 fibronectin fragments.<sup>111</sup> The signalling proteins downstream of  $\alpha 5\beta 1$  have since been identified. In short,  
298 PKC $\delta$  activation of proline-rich tyrosine kinase 2 (PYK2) and downstream activation of the MAP kinases  
299 ERK1/2, JNK1/2, and P38 $\alpha$  leads to heightened activity of NF- $\kappa$ B and activator protein-1 (AP-1) transcription  
300 factors.<sup>111-114</sup> This signalling also requires the production of reactive oxygen species and the presence of  
301 active Rac1.<sup>115 116</sup> It has also been noted that MAP kinases are required for stimulation of nitric oxide (NO),

302 MMP3, and MMP13 production, which further potentiate the progression to OA<sup>117-119</sup> Compression or shear  
303 stress activate ERK1/2 and P38 MAPK contributing to an increase in the expression of proinflammatory  
304 cytokines and molecules whilst also regulating the expression of mechanoresponsive anabolic genes (Figure  
305 3).<sup>120</sup> While therapeutic inhibition of MAPKs holds great potential in slowing the progression of OA, there  
306 remain safety concerns over the use of general MAPKs inhibitors in humans.<sup>121</sup> Considering the involvement  
307 of MAPKs within a complex signaling network, it is likely that a system offering long-term feedback for the  
308 controlled delivery of therapeutics will be required. Furthermore, targeting the deleterious processes  
309 downstream of MAPK activation, such as the mechano-inflammation mediators discussed below, may be a  
310 more attractive therapeutic option. Aside from this, the use of targeted, biomaterial-based approaches,  
311 utilized typically in tissue engineering applications may enable increased specificity and efficacy of selective  
312 modulation of MAPKs in a therapeutic manner. For example, the application of highly versatile functionalized  
313 scaffolds, which have previously demonstrated success in modulating c-Jun N-terminal kinase 3 (JNK3) for  
314 enhancing the osteogenic potential of mesenchymal stem cells, might provide the basis as a platform for  
315 targeted regulation of MAPK signaling pathways in other tissues such as cartilage.<sup>122</sup>

316

### 317 ***Mechano-inflammation and the NF- $\kappa$ B signalling pathway***

318 Aside from the well-known cytokine-mediated activation of the NF- $\kappa$ B signaling, NF- $\kappa$ B activation can also be  
319 regulated by physical forces in chondrocytes. For example, low magnitude mechanical strain blocks nuclear  
320 translocation of NF- $\kappa$ B, preventing upregulation of proinflammatory genes<sup>123</sup>. Conversely, high magnitude  
321 mechanical strain, representative of that experienced in injury, induces transactivation of NF- $\kappa$ B signaling  
322 complex and expression of proinflammatory genes, cartilage destruction and inhibition of ECM synthesis<sup>124</sup>.  
323 These findings indicate a central role for mechano-inflammation in the progression of OA and perhaps more  
324 importantly open the door to a number of promising therapeutic targets.

325 A well described mechano-inflammatory pathway involves activation of the TGF $\beta$ -activated kinase 1  
326 (TAK1), upstream of the P38 MAPK, c-Jun N-terminal kinase (JNK) and NF- $\kappa$ B signaling (Figure 3).<sup>125</sup> Of  
327 particular note, is that although TAK1 can be activated by inflammatory cytokines and TLR ligation, the  
328 pattern of ubiquitination of TAK1 observed is distinct from that seen following cytokine stimulation.<sup>126</sup>  
329 Recently, GREMLIN-1, a secreted BMP agonist, has also been identified as a mediator of NF- $\kappa$ B signaling  
330 following excessive mechanical loading in chondrocytes. Inhibition of VEGFR2 or NF- $\kappa$ B attenuated  
331 GREMLIN-1 induced pro-inflammatory and catabolic activity. Moreover, GREMLIN-1 antibody or  
332 chondrocyte-specific knockdown suppresses OA development *in vivo*, while the delivery of recombinant

333 GREMLIN-1 accelerates this process. Further investigation revealed that mechanically loaded GREMLIN-1  
334 production occurs through the Rac1-ROS-NF- $\kappa$ B pathway (Figure 3).<sup>127</sup>

335 Inflammation predisposes chondrocytes to become hypersensitive to injurious levels of mechanical  
336 loading as a result of IL-1 $\alpha$  induced upregulation of Piezo1 and subsequent increased basal Ca<sup>2+</sup> levels.<sup>128</sup>  
337 Interestingly, the presence of IL-1 $\alpha$  also increased chondrocyte deformation in response to the same loading  
338 magnitude due to F-actin rarefication. Further to these findings, a signaling mechanism from the IL-1 receptor  
339 type I (IL-1RI) complex on the cell membrane via MKK3/6 to P38 MAPK has been delineated through  
340 phosphorylation of P38 to the nuclear signaling of the transcription factor CREBP1, which together with ATF2  
341 and HNF4 $\alpha$  up-regulates PIEZO1 (Figure 3). This 'feed forward' mechanism, as described by the authors,  
342 indicates mechano-inflammation contributes to the maladaptive reprogramming of chondrocytes and  
343 provides a rational set of mechanotransduction informed targets for therapeutic approaches to OA.<sup>128</sup>

344 In the same study, TRPV4 expression levels and function were not altered by the presence of IL1 $\alpha$ ,  
345 suggesting that inflammation has a selective effect on the expression of cell mechanosensory machinery.  
346 However, TRPV4 has also been identified as a key mechanoreceptor involved in mechano-inflammation.  
347 Recent studies investigating how ECM viscoelasticity modulates the function of healthy and OA chondrocytes  
348 has shown that under static conditions, chondrocytes interact with the ECM of fast- and slow-relaxing alginate  
349 hydrogels, regulating their volume and phenotype.<sup>8</sup> In fast-relaxing gels, chondrocyte cell volume expands  
350 and ECM expression is upregulated, while the opposite holds true for slow-relaxing gels. While inflammation  
351 predisposes cells to mechanical stress, the reverse has also been observed where cells cultured in slow-  
352 relaxing gels undergo a proinflammatory phenotypic shift, making the cells more sensitive to extrinsic  
353 inflammatory cues.<sup>8,128</sup> Mechanistically, one mechanism through which chondrocytes sense and respond to  
354 changes in matrix viscoelasticity is through the TRPV4-GSK3 $\beta$  molecular axis. Treatment of cells in slow-  
355 relaxing gels with a TRPV4 selective inhibitor reduced inflammation and shifted the cells towards the  
356 phenotype observed in fast-relaxing gels. Similarly, treatment of cells cultured in fast-relaxing gels with a  
357 TRPV4 activator, resulted in an increase in intracellular Ca<sup>2+</sup>, GSK3 $\beta$  phosphorylation and a subsequent  
358 increase in inflammation (Figure 3).<sup>8</sup> It is interesting to note that a TRPV4-phosphatidylinositol 3-kinase  
359 (PI3K)/ Akt-p27Kip1 signalling axis has been demonstrated to control tumour cell (MDA-MB-231)  
360 proliferation, which is promoted in fast relaxing hydrogels but arrested in slow relaxing gels.<sup>129</sup> In  
361 chondrocytes, cell confinement in fast relaxing viscoelastic hydrogels has been reported to enhance  
362 proliferation, ECM production, and anabolic gene expression. Furthermore, in this study restricted cell  
363 expansion was also shown to induce IL-1 $\beta$  signalling, highlighting the interplay between cell expansion and

364 OA progression.<sup>130</sup> Unlike healthy chondrocytes, which can sense and transduce changes in ECM  
365 viscoelasticity, OA chondrocytes are unable to do so. Interestingly, treatment of OA chondrocytes with a  
366 TRPV4 inhibitor failed to change Ca<sup>2+</sup> levels suggesting a dysregulation of the TRPV4-GSK3 $\beta$  molecular axis  
367 in OA chondrocytes.<sup>8</sup> While TRPV4 plays a central role in responding to mechanical signals in healthy  
368 chondrocytes, its impairment in OA chondrocytes may limit its use as a therapeutic target (at least in the later  
369 stages of OA). Such findings highlight the importance of not only understanding the mechanism of drift in  
370 chondrocyte phenotype but also the timing of the molecular events governing this shift and will be invaluable  
371 in determining treatment strategies.

372

### 373 ***The WNT signalling pathway***

374 WNT signalling has established roles in embryonic development, tissue homeostasis, growth and is  
375 implicated in the onset and progression of various pathologies (specifics reviewed in <sup>131</sup>). In cartilage, WNT  
376 activity is essential for cartilage homeostasis, however controlled activity is required with a moderate amount  
377 of WNT activity shown to be essential for chondrocyte proliferation while excessive activity contributes to  
378 hypertrophy and increased expression of MMPs. In OA, the expression of WNT pathway members is  
379 dysregulated, increasing the expression of catabolic enzymes.<sup>132</sup> Mechanical injury leads to the upregulation  
380 of Frizzled-related protein (*FRZB*), a WNT-binding protein.<sup>133</sup> Meanwhile, knockout of *FRZB* leads to an  
381 increase in MMP expression and the accumulation of  $\beta$ -catenin in IL-1 $\beta$  stimulated chondrocytes. A  
382 microarray and systematic analysis revealed distinct differences between healthy and injured cartilage  
383 including the up-regulation of WNT-16, downregulation of *FRZB*, upregulation of WNT target genes, and  
384 nuclear localization of  $\beta$ -catenin. Furthermore, WNT-16 and  $\beta$ -catenin were up-regulated in areas of the same  
385 joint that had moderate to severe OA compared to preserved cartilage areas.<sup>134</sup> In a mouse model of OA,  
386 both protein and mRNA levels were also up-regulated, however, WNT16 deficient mice presented with more  
387 severe OA suggesting a homeostatic role. Interestingly, WNT16 deficient mice failed to up-regulate lubricin  
388 (*PRG4*), a low friction proteoglycan and chondroprotective agent.<sup>135</sup> The WNT signaling pathway thus  
389 presents potential therapeutic targets for the treatment of OA.<sup>132,136,137</sup> However, the involvement of WNT  
390 signaling in so many important biological processes makes targeting these pathways a daunting task. Any  
391 such intervention should aim to fine tune WNT signaling activity (Reviewed further by <sup>138</sup>). Recent strong  
392 performance of Lorecivint (SM04690), a WNT pathway modulator, in Phase 1 (NCT02095548) and Phase  
393 2 (NCT02536833, NCT03122860) clinical trials is encouraging and demonstrated safety and efficacy in knee  
394 OA patients, with significant improvements observed compared to placebo.<sup>139,140</sup> Lorecivint, inhibits the

395 activity of CDC-like kinase enzymes (CLKs), in particular CLK2 and dual-specificity tyrosine phosphorylation-  
396 regulated kinases enzymes (DYRK), specifically DYRK1A, enhancing chondrogenesis, chondrocyte function,  
397 and anti-inflammation (Figure 3).<sup>141</sup> Another promising therapeutic is DOT1-Like Histone Lysine  
398 Methyltransferase (DOT1L), which has been shown limit WNT activation. DOT1L appears to have a  
399 chondroprotective role in cartilage, with intra-articular delivery of a DOT1L inhibitor found to trigger  
400 development of OA (Figure 3).<sup>142-144</sup>

401

### 402 ***YAP/TAZ signalling pathway***

403 The transcriptional cofactors Yes-associated protein (YAP) and transcriptional coactivator with PDZ-binding  
404 motif (TAZ) form a key mechanosignalling complex and are involved in regulating chondrogenesis,  
405 chondrocyte maturation, and hypertrophy.<sup>145</sup> YAP/TAZ activity is tightly regulated by biochemical and  
406 mechanical regulation. Biochemically, they are members of the Hippo pathway, which can be activated by  
407 cadherin-cadherin interactions and leads to YAP phosphorylation and retention in the cytoplasm, where it  
408 cannot act to influence transcription. This regulation demonstrates that YAP/TAZ activity can be controlled  
409 by cell structure and polarity, cell-ECM interactions, and physical cues from the microenvironment and directly  
410 converted into gene expression profiles, adapting cell phenotypes rapidly. In complex or in vivo 3D  
411 environments, however, YAP/TAZ regulation is not fully understood and responses divergent from well-  
412 established 2D responses have been reported.<sup>146,147</sup> During chondrogenesis of MSCs in vitro, YAP is  
413 downregulated.<sup>148</sup> YAP also inhibits terminal chondrocyte maturation and hypertrophy by suppressing type  
414 X collagen expression (COL10A1) through interacting with runt-related transcription factor 2 (RUNX2), an  
415 important regulator of chondrocyte hypertrophy and osteogenesis.<sup>145</sup> In OA, deletion of YAP promotes  
416 cartilage disruption, while proinflammatory cytokines typically upregulated in the OA joint (IL-1 $\beta$ , TNF- $\alpha$ ) drive  
417 the destruction of YAP through TAK1-mediated phosphorylation. YAP also interacts with TAK1 and  
418 attenuates NF- $\kappa$ B signalling by inhibiting substrate accessibility, which establishes a reciprocal antagonism  
419 between YAP/TAZ and NF- $\kappa$ B, important in regulation of proinflammatory responses in OA (Figure 3).<sup>10</sup>

420

### 421 ***Central energy metabolism and activity metabolites***

422 Metabolism has a key role in OA progression and recent studies have begun to reveal links between  
423 chondrocyte mechanotransduction and metabolic pathways.<sup>149</sup> Central energy metabolism pathways  
424 (glycolysis, the pentose-phosphate pathway (PPP), and the Krebs/TCA cycle etc.) are how cells harvest  
425 energy (e.g., ATP) generating the precursors to non-essential amino acids.<sup>150</sup> There is now strong evidence



426 that mechanosignalling can regulate cell metabolism and that metabolic processes in healthy and OA  
427 chondrocytes respond differently to mechanical stimuli. For example, in OA chondrocytes cyclic loading  
428 reduces phosphorylation of AKT, a regulator of Forkhead box O (FoxO) signalling in energy homeostasis.<sup>151</sup>  
429 Conversely, mechanical stimulation induces AKT phosphorylation in healthy cells.<sup>152</sup> These different  
430 metabolic responses have implications for downstream anabolic responses to mechanical loading observed  
431 in healthy cells, fuelled by a glycolytic energy flux that is reduced in OA.<sup>153</sup> Investigating the effect of  
432 mechanically induced changes on the cellular metabolome can enable the identification of metabolites  
433 involved in mediating cell mechanotransduction and phenotypes, opening the possibility of harnessing these  
434 'activity metabolites' to control cell behaviour or developing chemical analogs with enhanced therapeutic  
435 action.<sup>154-156</sup> Metabolomics data obtained to date has highlighted the role of various signalling pathways  
436 associated with mechanotransduction. Considering the multifactorial nature of OA and the distinct shift in  
437 chondrocyte metabolism in disease, it is likely that further elucidation of the role of central energy metabolism  
438 in mechanotransduction will yield promising therapeutic targets by comparing mechanically-induced  
439 metabolite expression in both healthy and OA chondrocytes.<sup>154,155</sup>

440

441

## 442 **Future Directions**

443 Physical therapy is commonly used in the non-pharmacological treatment of OA, albeit without a  
444 comprehensive understanding of the underlying cellular mechanosensory and signaling mechanisms at  
445 play.<sup>107</sup> Understanding mechanosignalling holds the key for the development of therapeutics that control  
446 cellular responses, halt disease progression, and enable regeneration of the cartilage tissue. While promising  
447 DMOADs have emerged in recent years (e.g., COX-2 inhibitors, corticosteroids, IL-1 $\beta$  inhibitors, TNF- $\alpha$   
448 inhibitors etc.), these have not proved to be as effective as hoped and a rethinking of how we develop  
449 therapeutics for OA is required. A good starting point may be the repurposing of selective small molecule  
450 inhibitors (SMIs) that have shown success in blocking mechanosignalling pathways in other mechanosensate  
451 cells/ tissues. For example, WRG-28 specifically inhibits the receptor-ligand interactions of discoidin domain  
452 receptor 2 (DDR2) in tumours, but aberrant DDR2 activation has also been implicated in OA.<sup>157</sup> The  
453 continuing development of advanced cartilage-on-a-chip models, capable of recapitulating *in vivo*-like  
454 physiological and pathological mechanical and biochemical cues in higher-throughput systems, will provide  
455 valuable methods for rapid and accurate screening of prospective DMOADs prior to *in vivo* testing.<sup>158</sup>

456 In addition to the physical impediments to developing and delivering successful DMOADs (e.g.,  
457 tissue location, dense ECM, rapid drug clearance), there is an intricate link between mechanosignalling and  
458 critical catabolic-anabolic signalling axes driving the progression of OA. While research to date largely  
459 focuses on controlling one specific parameter (e.g., matrix stiffness, growth factor presentation, inflammation,  
460 mechanical stimulation, biomaterial degradation etc.), this approach often overlooks this complex interplay  
461 between stimuli. However, researchers should not despair at the overwhelming complexity of these pathways  
462 as collectively we continue to make advancements in our therapeutic toolbox. For example, recent  
463 development of biomaterials capable of regulating a combination of these factors simultaneously has enabled  
464 acquisition of valuable insights into this signalling interplay. For example, investigations into the role of  
465 several mechanosignalling pathways (integrin  $\alpha 5\beta 1$ , YAP, SMAD/TGF $\beta$ , MAPKs and WNT) and their  
466 involvement in regulating the differentiation of hMSCS cultured on articular or hypertrophic promoting  
467 hydrogels with cyclic compression. This approach revealed a role for down-regulation of WNT signaling to  
468 promote articular-like chondrocyte phenotypes in soft matrices and confirmed YAP-regulation of hypertrophy  
469 in stiff matrices.<sup>145,159</sup> The application of -omics analysis with such platforms to map cellular and molecular  
470 responses to tightly controlled biomechanical stimuli (mechanomics) will provide even greater insight into  
471 responses to specific stimuli.<sup>160</sup>

472 Another important consideration in mechanotherapeutics is timing of intervention. As the articular  
473 joint tissue heals, the needs of the tissue evolve, adding a further degree of complexity. Further to this,  
474 therapies for OA, a disease that is intricately linked to the aging process, may require sustained drug  
475 administration over a long time-period, whilst maintaining the delicate anabolic-catabolic balance. It is also  
476 likely that OA patients will show an increase in co-morbidities as they age, which may further complicate  
477 treatment. To overcome these challenges, significant advancements have been made in developing  
478 cartilage-specific drug delivery strategies. For example, developments in advanced therapeutic approaches  
479 such as gene therapy for the delivery of plasmid (p)DNA or RNA-based therapeutics (siRNA, miRNA) may  
480 help overcome issues with target specificity, safety and bioavailability. In recent years, advances in vector  
481 technologies and a greater understanding of the mechanisms of action have led to a surge in the development  
482 of gene therapy approaches. The planned FDA Phase 3 clinical trials (TGC12301, TGC15302) of  
483 INVOSSA™ (Kolon TissueGene), for the delivery of TGF $\beta 1$ , will be observed closely by researchers, with a  
484 successful outcome potentially opening a new era of gene therapy for OA. The potential of siRNAs has been  
485 demonstrated through knockdown of modulators of mechano-inflammation including WNT/  $\beta$ -catenin, NF- $\kappa$ B  
486 and p38 MAPK<sup>161,162</sup> (reviewed recently in <sup>163</sup>). MicroRNAs (miRNAs - small single-stranded non-coding

487 RNAs) are highly potent post-transcriptional regulators, as one miRNA can exert an effect on multiple  
488 mRNAs. Several miRNAs have been shown to be mechanically-regulated in chondrocytes, with alterations  
489 in miR expression associated with OA and with different cartilage zones subjected to different degrees of  
490 mechanical loading.<sup>164-168</sup> miRNA profiling of OA cartilage has revealed unique miRNA signatures and  
491 several miR's have been identified as potential therapeutic targets.<sup>169</sup> One promising candidate, for example,  
492 is miR-365, which is upregulated with cyclical loading of chondrocytes and in OA, regulates cell hypertrophy  
493 through a mechanism involving NF- $\kappa$ B and HDAC4.<sup>170</sup> Itself a potent inhibitor of chondrocyte hypertrophy and  
494 MMP expression, HDAC4 activity is inhibited by miR-365 and MMP13 and type X collagen expression  
495 increased. Inhibition of miR-365 was able to attenuate this upregulation.<sup>166,170</sup> Conversely, miR-222 is down-  
496 regulated in OA chondrocytes and is implicated in regulating cartilage destruction and MMP-13 expression.  
497 Intra-articular delivery of miR-222 to mouse destabilised medial meniscus models recovers cell number and  
498 significantly reduces cartilage destruction.<sup>171,172</sup> More recently, miRNAs regulated by different loading  
499 conditions has led to the discovery of several miRs (miR-199b-5p, miR-1229-5p, miR-1275, miR-4459, miR-  
500 6891-5p, and miR-7150) which were only affected under catabolic loading conditions.<sup>173</sup> These systematic  
501 approaches investigating diverse loading conditions in both healthy and OA cells is likely to lead to further  
502 development of therapeutic avenues in this area.<sup>174</sup>

503           Mechanoresponsive smart biomaterials that leverage the mechanical environment of the joint during  
504 regeneration can facilitate drug delivery in sync with the needs of the tissue, ultimately enhancing the  
505 therapeutic process (Figure 4). For cartilage applications, a suite of mechanically-activated microcapsules  
506 (MAMCs) with varying thresholds of mechanoactivation capable of releasing TGF $\beta$ 3 have been developed.<sup>175</sup>  
507 Using this MAMC system to deliver anti-inflammatory agents was demonstrated to successfully reduce matrix  
508 degradation in engineered cartilage constructs treated with IL1 $\beta$  (Figure 4).<sup>12</sup> However, issues remain  
509 surrounding prolonging delivery *in vivo* in these systems over timescales suitable for cartilage regeneration  
510 and fine-tuning release profiles to mechanical inputs. In order to overcome these limitations, researchers  
511 have begun to develop autonomous mechanotherapeutics, which can respond in real-time to the changing  
512 microenvironment, thus overcoming issues with long-term integration, target specificity, timing, homeostatic  
513 maintenance and repeated administration. Recently, for example, through deconstructing the signaling  
514 networks downstream of TRPV4 activation, a synthetic TRPV4-responsive gene circuit was developed, which  
515 was shown to be effective as an autonomously regulated drug delivery system capable of producing  
516 interleukin-1 receptor antagonist in response to mechanical loading (Figure 4).<sup>176</sup> While only used for the  
517 mechanical activation of TRPV4 and the delivery of a specific anti-inflammatory, the framework of this system

518 opens the door to other mechanoreceptors and signalling pathways, allowing for a new generation of  
519 mechanotherapeutics. The development of such mechanically responsive biomaterials and closed-loop drug  
520 delivery systems may be the key in maintaining treatment efficacy in the changing environment in the joint  
521 during regeneration.

522

### 523 **Conclusion**

524 Mechanical stimuli are a critical environmental factor in maintaining joint homeostasis. How chondrocytes  
525 sense and respond to these mechanical forces determines cellular phenotype, regulates inflammation and  
526 tightly controls the anabolic-catabolic axis required for cartilage health. Chondrocytes are equipped to  
527 respond to these forces through a variety of mechanosensory mechanisms and signalling. Altered  
528 mechanical forces, as a result of trauma or a reduced capacity to withstand normal loading conditions,  
529 regulates cell processes central to OA pathology, thus providing a number of effectors which can be targeted  
530 to uncouple pathological feedback loops. Coupling these targets with advanced drug delivery systems  
531 ranging from gene therapy to mechanosensitive biomaterials offers great promise in the development of safe  
532 and effective treatments for OA.

533

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543

### 544 **Competing Interests**

545 The authors declare no competing interests.

546

547 **Figure 1 Articular cartilage composition and structure.** Schematic representation of articular cartilage  
548 composition and structure in healthy and osteoarthritic tissue states. The structure of articular cartilage can  
549 be divided into four distinct zones (superficial, middle, deep and calcified). Each zone exhibits characteristic  
550 composition and organization. The ECM composition and architecture represent the forces experienced  
551 within these zones. Chondrocytes and type II collagen fibres are orientated transversely in the superficial  
552 zone, enabling the dispersion of shear forces during articulation. The presence of lubricin/proteoglycan 4  
553 (PRG4) within this zone further facilitates lubrication of the joint. Within the middle zone, type II collagen  
554 fibres resist compressive and shear forces from a number of directions, exhibited by the random arrangement  
555 of the fibres. Thick collagen fibres arranged perpendicular to the articulating joint surface in the deep zone  
556 resist compressive loads. High concentrations of proteoglycan in this zone enable water retention. The matrix  
557 in which chondrocytes reside also differs in composition and structure and can be divided into three regions  
558 moving from the chondrocyte outwards – the pericellular matrix (PCM), territorial matrix (TM) and the  
559 interterritorial matrix (ITM). The PCM, characterized by the presence of type VI collagen, surrounds the  
560 chondrocyte and has a significant influence on chondrocyte mechanotransduction. The PCM also contains  
561 other important components (i.e. hyaluronan, biglycan, fibronectin). The PCM integrates with the TM, a region  
562 characterized by tightly packed fibrillary collagen and proteoglycan. The outermost region, termed the ITM,  
563 is used to refer to the bulk tissue ECM. While the integrity of the ECM as a whole plays a significant role in  
564 the transmission of forces across the tissue, each specific zone determines the type of loading experienced  
565 by a chondrocyte, influencing the cell response.

566

567 **Figure 2 Chondrocyte mechanosignalling.** An illustrative overview of key mechanosensing mechanisms  
568 in chondrocytes.(A) Indirect mechanosensing. On deformation, extracellular matrix sequestered growth  
569 factors including fibroblast growth factor (FGF), bone morphogenetic protein (BMP) and transforming growth  
570 factor (TGF) activate cell surface receptors. FGF binds to FGF receptors (FGFRs) and phospholipase C $\gamma$   
571 (PLC $\gamma$ ) is activated by binding to the kinase domains of FGFRs and in turn stimulates protein kinase C (PKC)  
572 activity and activates downstream MAP kinases. FGF receptor ligand binding also activates growth factor  
573 receptor-bound protein 2 (GRB2), activating RAS, resulting in activation of extracellular signal regulated  
574 kinase (ERK1/2). ERK1/2 translocates to the nucleus and impacts the activity of numerous transcription  
575 factors. BMPs and TGFs bind to heterodimer BMP and TGF cell surface receptors (BMPR, TGFR). In the  
576 SMAD signalling pathway either SMAD 1/5/8 (BMPRs) or SMAD 2/3 (TGFRs) are phosphorylated and  
577 activated on ligand-receptor binding, recruiting SMAD4 and translocating to the nucleus and impacting

578 transcription. Non-SMAD signalling pathways are activated through TGF $\beta$  activated kinase (TAK1), which  
579 can activate JUN N-Terminal Kinase (JNK), P38 Mitogen Activated Protein Kinase (P38) and Nuclear Factor  
580  $\kappa$ B (NF- $\kappa$ B). (B) Direct mechanosensing. Integrin activation can trigger biochemical signal transduction and  
581 direct mechanical deformation of the cell through cytoskeletal contraction. On integrin binding, SRC kinase  
582 and focal adhesion kinase (FAK) recruitment result in GRB2 binding and downstream activation of ERK1/2  
583 and JNK signalling. Integrin binding also triggers PI3K/ AKT pathway activation through Integrin Linked  
584 Protein Kinase (ILK). Mechanically regulated ion channels such as Transient Receptor Potential Cation  
585 Channel 4 (TRPV4) and Piezo Type Mechanosensitive Ion Channel Component 1/ 2 (PIEZO1/2) drive Ca<sup>2+</sup>  
586 influxes into cells, activating numerous downstream signalling pathways. (C) Primary cilium-mediated  
587 mechanotransduction. Primary cilia house high levels of multiple mechanosensory receptors and channels  
588 involved in direct and indirect mechanosensing. On mechanical stimulation, for example through deflection  
589 when experiencing fluid flow, these are activated, resulting in downstream activation of multiple signalling  
590 pathways as elsewhere in the cell.

591  
592 **Figure 3 Mechano-inflammation signaling in chondrocytes in osteoarthritis.** Mechano-inflammation in  
593 OA involves several key signaling pathways which can be activated by both inflammatory cytokines and/or  
594 mechanical stimuli. Mechanical regulation of pathway activity controls both downstream anabolic and  
595 catabolic processes offering a number of promising therapeutic targets which can halt the progression of OA  
596 while concomitantly stimulating anabolic repair. Activation of mechano-inflammatory signaling contributes to  
597 increased inflammatory gene expression, alterations in cytoskeletal phenotype, energy homeostasis and an  
598 increase in catabolic mediators. Key mediators within mechano-inflammation include TGF $\beta$ -activated kinase  
599 1 (TAK1), YAP/TAZ, Nuclear Factor  $\kappa$ B (NF- $\kappa$ B), JUN N-Terminal Kinase (JNK), P38 Mitogen Activated  
600 Protein Kinase (P38) and downstream mediators of the WNT signaling pathways. TAK1 activation occurs  
601 upstream of the P38 MAPK, c-Jun N-terminal kinase (JNK) and NF- $\kappa$ B. Inflammatory cytokines drive the  
602 destruction of YAP through TAK1-mediated phosphorylation, while YAP can also interact with TAK1  
603 attenuating NF- $\kappa$ B. GREMLIN-1 exerts a pro-inflammatory effect through the GREMLIN-1-VEGFR axis.  
604 Induction of GREMLIN-1 as a result of excessive mechanical loading occurs via the Rac1-ROS-RelA/p65  
605 axis and NF- $\kappa$ B signaling. Mechano-inflammation predisposes chondrocytes to a state of hypersensitization,  
606 rendering them susceptible to inflammatory and mechanical stimuli present within normal physiological  
607 ranges. IL-1 $\alpha$  induces the upregulation of Piezo Type Mechanosensitive Ion Channel Component (PIEZO1),  
608 increased calcium (Ca<sup>2+</sup>) levels and contributes to F-actin rarefication via the transcription factors CREBP1,

609 ATF2 and HNF4 $\alpha$ . Chondrocytes sense and respond to changes in matrix viscoelasticity through the  
610 Transient Receptor Potential Cation Channel 4 (TRPV4)-GSK3 $\beta$  axis, where TRPV4 activation, either  
611 pharmacologically or through culturing of cells on slow-relaxing gels, results in increased Ca<sup>2+</sup>, GSK3 $\beta$   
612 phosphorylation and increased inflammation. Therapeutic targeting of mechanoinflammation and its signaling  
613 pathways holds promising potential. Lorecivivint, a WNT pathway modulator, inhibits CDC-like kinase  
614 enzyme (CLK2) and dual-specificity tyrosine phosphorylation-regulated kinases enzymes (DYRK1A) activity  
615 enhancing chondrogenesis and anti-inflammation. Additionally, DOT1-Like Histone Lysine Methyltransferase  
616 (DOT1L) interacts with SIRT1 preventing Wnt pathway hyper-activation, maintaining cartilage homeostasis.  
617

618 **Figure 4 Mechano-responsive therapeutics for the treatment of osteoarthritis.** Mechanotherapeutic  
619 approaches aim to take advantage of the dynamic physical stimuli present in the joint in order to deliver  
620 biomolecules. Approaches including drug loaded cross-linkable block copolymer hydrogels and tethered  
621 drug-filled depots enable delivery of biomolecules in a spatio-temporally controlled manner. Mechanically  
622 activated microcapsules (MAMCs) can be tailored to rupture in response to specific loading conditions  
623 enabling delivery of therapeutics in a controllable manner based on the specific needs of the tissue at any  
624 given time. Development of MAMCs encapsulating chondrogenic therapeutics (TGF $\beta$ ) or anti-inflammatory  
625 agents (interleukin-1 receptor antagonist) have shown promising potential in cartilage regeneration. Further  
626 advancements within the fields of synthetic biology and tissue engineering have enabled the reprogramming  
627 of mechanotransduction and signaling pathways for the development of autonomously regulated drug  
628 delivery systems which can respond in real-time to the ever-changing mechanical microenvironment of the  
629 joint enabling enhanced tissue repair. A comprehensive understanding of the underlying signaling networks  
630 downstream of mechanoreceptor activation can be used for the development of synthetic gene circuits  
631 responsive to mechanical loading. The development of a synthetic TRPV4-responsive gene circuit enables  
632 autonomous production of the anti-inflammatory agent interleukin-1 receptor antagonist in response to  
633 mechanical loading.

634

635 **BOX 1 | MECHANO-INFLAMMATION IN OSTEOARTHRITIS**

636 Mechano-inflammation can be described as the inflammatory response to mechanical injury. Beyond wear  
637 and tear, excessive mechanical loading of the cartilage activates receptors and signalling pathways that  
638 result in the production of the catabolic enzymes that drive degradation of the functional cartilage ECM.  
639 Evidence from OA and other forms of arthritis also indicates that mechanical strain is important in determining  
640 the localisation of inflammation and tissue degradation.<sup>40,177</sup> Deletion or inhibition of mechanically induced  
641 proteases, or the inflammatory signalling pathways that control them, prevents OA progression in animal

642 models, even when joints are destabilised.<sup>1,40</sup> Similarly, progression of OA is prevented when joints are  
643 immobilised following induction of OA or when superficial zone chondrocytes are specifically destroyed prior  
644 to joint destabilisation.<sup>2,4</sup> Mechano-inflammation involves several key signalling pathways including TGF $\beta$ ,  
645 P38, JNK, YAP/TAZ and NF- $\kappa$ B. TGF $\beta$ -activated kinase 1 (TAK1), which can be activated by both  
646 inflammatory cytokines and mechanical stimuli, appears to be involved in a number of these responses.<sup>178</sup>  
647 TAK1 mediates mechanical activation of MAPK cascades and is central to YAP/TAZ anabolic activity and  
648 reciprocal inhibitory interaction with NF $\kappa$ B.<sup>10</sup> It follows then that control of mechano-inflammation in the OA  
649 joint has the potential to both control catabolic processes and promote anabolic repair processes.  
650 Interestingly, along with magnitude, duration and frequency of force applied to the joint, the type of loading  
651 experienced by chondrocytes situated in the different zones of the cartilage appears to be significant in  
652 determining whether mechano-inflammation is activated, or anabolic processes are stimulated.<sup>2</sup> Targeting  
653 mechano-inflammation, either through restoration of a functional mechanical environment (e.g., by  
654 biomaterials) or by controlling key signalling mechanisms and receptors, might be one of the most promising  
655 strategies for improving the efficacy of OA therapies.

656

657

## 658 **BOX 2 | USE OF MECHANO-RESPONSIVE ‘SMART’ BIOMATERIALS IN CARTILAGE**

659 Mechano-responsive smart biomaterials can be designed to adapt and respond to the changing mechanical  
660 microenvironment of the joint during tissue restoration. By harnessing the constant dynamic stimuli present  
661 in the joint, mechano-responsive biomaterials can be used to deliver biomolecules in a spatio-temporally  
662 controlled manner (Figure 4).<sup>179</sup> Physical-based stimuli responsive drug delivery systems can deliver drugs  
663 in a controlled manner in response to compressive, tensile and shear forces.<sup>180</sup> For example, the use of  
664 mechano-responsive hydrogels, incorporating mechano-responsive drug depots enables the delivery of the  
665 anti-inflammatory drug dexamethasone in response to compressive forces applied to the gels.<sup>181</sup>  
666 Furthermore, the development of “smart” mechano-responsive biomaterials tailored to use specific  
667 mechanical cues present at various stages of the tissue regeneration process can deliver therapeutics  
668 sequentially based on the specific needs of the cells and tissue at any given time. The development of  
669 mechanically-activated microcapsules tuned to exhibit different rupture profiles enables specific drug release  
670 in a sequential manner using the different mechanical forces present throughout the healing process.<sup>12,175</sup>  
671 As our understanding of the receptors and signalling pathways involved in mechanotransduction increases,  
672 so too does the “degree of smartness” of mechanoresponsive approaches. In addition to responding to a  
673 particular physical force and delivering a specific drug, the use of advanced tissue engineering and synthetic  
674 biology approaches targeting mechanotransduction pathways involved in health and disease can enable  
675 “mechanobiological reprogramming” of cells for the creation of autonomous mechano-responsive constructs  
676 for enhanced tissue repair.<sup>176</sup>

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